

# Integrated flow sensor for in situ measurement and control of acoustic streaming in flexural plate wave micropumps

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## Abstract

This paper presents the design, fabrication, and characterization of a micromachined flow sensor, which is integrated onto the flexural plate wave (FPW) micropump. The flow sensor and the FPW micropump represent a complex microfluidic system that is able to control the fluid flow in the device. The system was designed using a commercial software package. The microfluidic system of a size of  $10 \times 10$  mm was fabricated using common fabrication techniques. The micropump is made of an aluminum, piezoelectric zinc oxide, polysilicon, and low-stress silicon nitride membrane with a typical thickness of  $1\text{--}3\text{ }\mu\text{m}$ . The thermal flow sensor consists of a polysilicon heater and polysilicon–aluminum thermopiles as temperature sensors. The cold junctions of the thermopiles are located in a new design that will avoid the drift effect of the flow sensor. The results show expected flow velocity–drive voltage characteristics. © 2000 Elsevier Science S.A. All rights reserved.

**Keywords:** Microfluidic system; Thermal flow sensor; Micro pump; Acoustic streaming

## 1. Introduction

Recently, microfluidic systems have emerged as an important research topic. Applications in microbiology and micro chemical analysis motivate the development of microfluidic systems that can control and deliver different fluids in nanoliter to microliter ranges. Numerous papers have been published focusing on the development of micro pumps and micro flow sensors. Some overviews of classical fluidic components can be found in Refs. [1–3]. Because of the backpressure dependency of the flow, there is a need to control the pumping performance in order to maintain a constant flow rate. Gass et al. reported a hybrid system that can regulate flow rate up to  $100\text{ }\mu\text{l}/\text{min}$  against backpressure up to 100 mbar [4]. Very few works presented a complex integrated system. Lammerink et al. [5] presented a system with an integrated thermal actuated micropump and a thermal flow sensor for flow rates on the order of  $10\text{ }\mu\text{l}/\text{min}$ . Pumps with flow rates on the order of  $1\text{ }\mu\text{l}/\text{min}$  were not reported.

In recent years, considerable attention has been focused on the use of flexural plate wave (FPW) devices for pumping fluids. This pumping principle enables the realization of an “active” micro channel and overcomes the high impedance encountered during delivery of fluid through channels.

Several papers have proven the possibility of using the FPW device as a micro-pump for submicroliter per minute flow rates [6–8]. The device presented in this paper consists of a flow sensor and an FPW micropump. The device is a first complex microfluidic system with an FPW pump.

Fig. 1 shows the structure of the microfluidic system described in this paper. The device consists of a rectangular flow channel that has a thin membrane on the bottom. The membrane is made of piezoelectric zinc oxide, aluminum, and low-stress silicon nitride, and has a typical thickness  $d_M$  of  $1\text{--}3\text{ }\mu\text{m}$ . With an FPW length  $\lambda$  of  $100\text{ }\mu\text{m}$ , the drive frequency  $f$  is in the range of  $3\text{--}5\text{ MHz}$ . Arrays of finger pairs placed at wavelength intervals termed interdigital transducers (IDTs) generate the plate waves. The flow sensor is integrated on the same membrane. The sensor consists of a polysilicon heater and temperature

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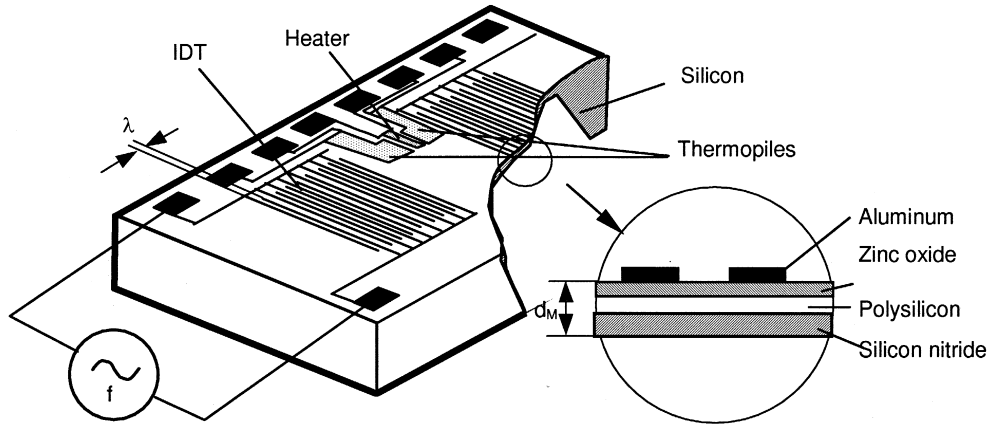


Fig. 1. The device with an FPW pump and a flow sensor.

sensors for detecting shifts of the temperature profile on the membrane.

## 2. Design of the device

### 2.1. Design of the FPW pump

The simulation utilizes the moving grid facilities of a commercial CFD software package (CFDRC Cooperation). A user library routine written in FORTRAN modifies the grid positions [9]. Essential parameters of the model such as the current time and grid positions can be specified from predefined constants and routines. The pressure field and the first-order velocity field of each time step are saved and used as the initial condition for the next time step. The vertical displacement  $\Delta z$  (perpendicular to the membrane), the horizontal displacement  $\Delta x$  (wave propagation direction), are given by:

$$\Delta z = A \sin(\omega t - kx), \quad (1)$$

$$\Delta x = \frac{A\pi d_M}{\lambda} \cos(\omega t - kx), \quad (2)$$

where  $A$  is the wave amplitude,  $\omega = 2\pi f$  is the angular frequency of the wave,  $k = 2\pi/\lambda$  is the wave number, and  $d_M$  is the membrane thickness. The time-averaged velocity field can then be calculated and depicted using MATLAB (Fig. 2). Details of the simulation results were described in Ref. [10].

In order to optimize the design of the FPW device for the best pumping performance, two parameters were investigated: the wave amplitude and the channel height.

Fig. 3 depicts the velocity profile and the peak velocity vs. the wave amplitude in a 50- $\mu\text{m}$  channel. The curve at the bottom represents the parabolic characteristic of the maximum velocity. Enlarging the wave amplitude increases the time-averaged velocity over the entire channel. The results here give an unequivocal behavior of the pumping performance that the flow rate varies as the

square of drive voltage, which is proportional to the wave amplitude. Therefore, the wave amplitude, and consequently the drive voltage, are the most important parameters for controlling the flow rate of the pump.

Results of the velocity profile in channel with different heights and an wave amplitude of 10 nm are shown in Fig. 4. The bottom curve is the peak velocity of each profile. It shows clearly that the maximum velocity stays constant with a channel height greater than the evanescent decay distance ( $\sim 20 \mu\text{m}$ ). Therefore, channels with heights greater than twice the evanescent decay distance of the acoustic field have equal volume flow rates.

The results also show that velocity increases substantially in channels with height less than the decay length of the acoustic evanescent. In such channels, the velocity has a parabolic profile with high peak velocities.

### 2.2. Design of the thermal flow sensor

The design of the thermal flow sensor is based on the analytical model described in [11]. With the temperature

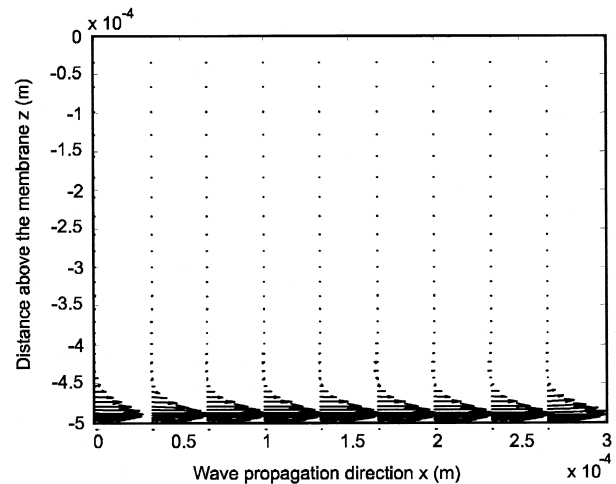


Fig. 2. Velocity field of the acoustic streaming in air (plate wave amplitude, 6 nm).

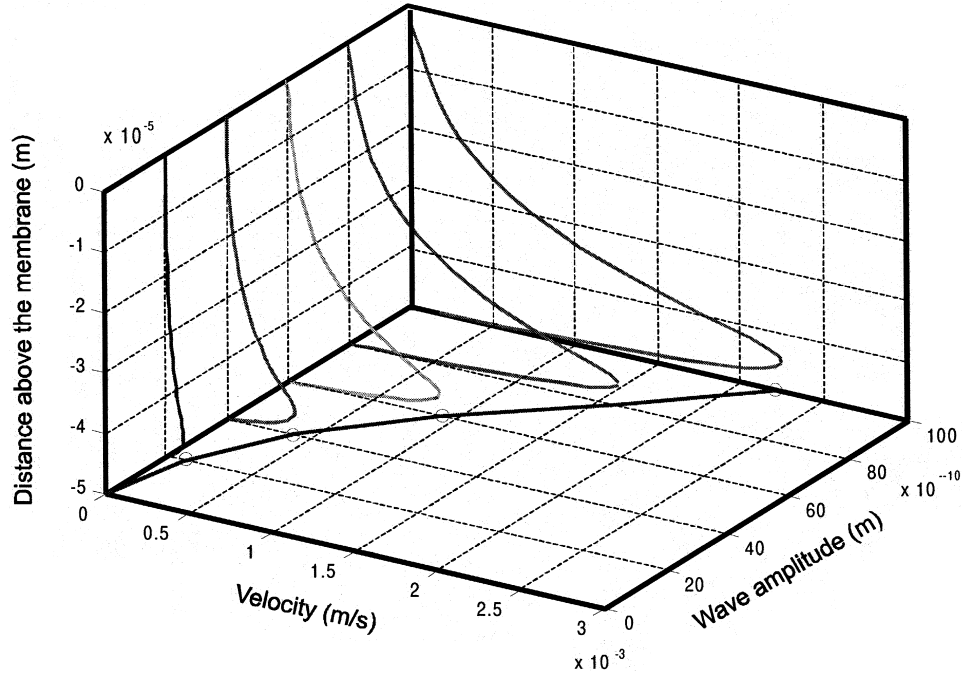


Fig. 3. Velocity profile of water over the channel height of 50  $\mu\text{m}$  driven by different wave amplitudes.

along the flow direction  $\vartheta$ , the average flow velocity  $v$ , the thermal conductivities of the membrane  $\lambda_M$  and of fluid  $\lambda_{FI}$ , the thermal diffusivity of fluid  $a_{FI}$ , the constant thickness of the thermal boundary layer  $\delta$ , the thickness of the membrane  $d_M$  and the distances of the temperature sensors to the heater upstream  $l_u$  and downstream  $l_l$ , we get the temperature difference  $\Delta\vartheta(v)$  between the temperature sensors:

$$\Delta\vartheta(v) = \vartheta_0 [\exp(\gamma_2 l_u) - \exp(-\gamma_1 l_l)] \quad (3)$$

with:

$$\gamma_{1,2} = \frac{v \pm \sqrt{v^2 + 16 a_{FI}^2 \kappa / \delta^2}}{4 a_{FI} \kappa} \quad (4)$$

The dimensionless factor:

$$\kappa = \frac{1}{2} + \frac{\lambda_M d_M}{\lambda_{FI} \delta} \quad (5)$$

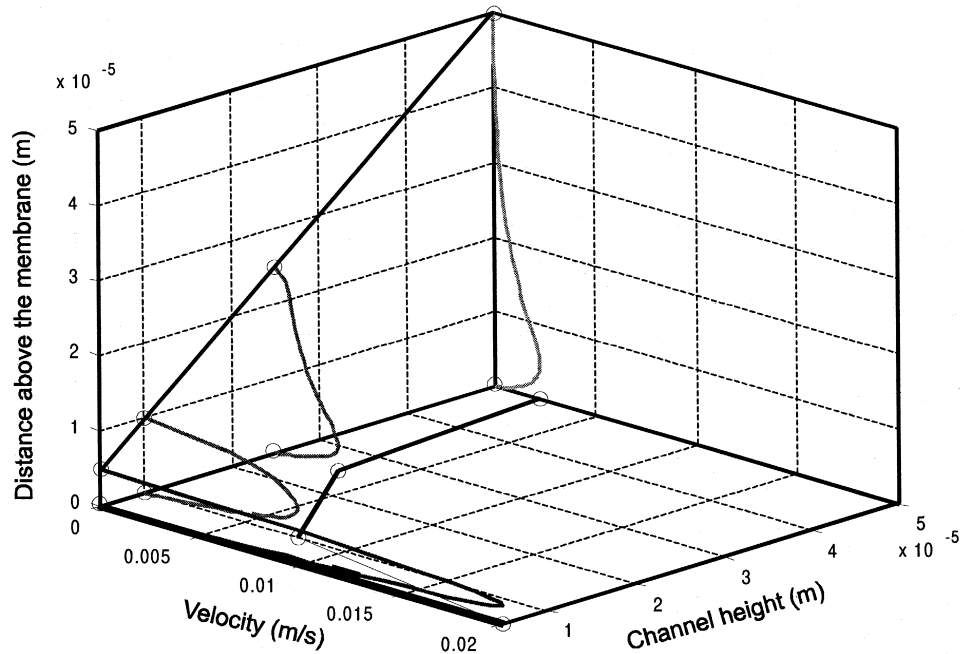


Fig. 4. Velocity profile of water with different channel heights driven by a wave amplitude of 10 nm.

describes the influence of the diaphragm material on the heat balance. The heater temperature at a constant heat power  $P$  is calculated with:

$$\vartheta_0 = \frac{P}{\lambda_{FI} b_H \left[ l_H / \delta + \sqrt{(v^2 \delta^2) / (4 a_{FI}^2) + 4 \kappa} \right]} \quad (6)$$

Results of this model and former investigations [12] show that the sensor signal is proportional to a small flow rate, which is the case of the acoustic streaming in the FPW pump.

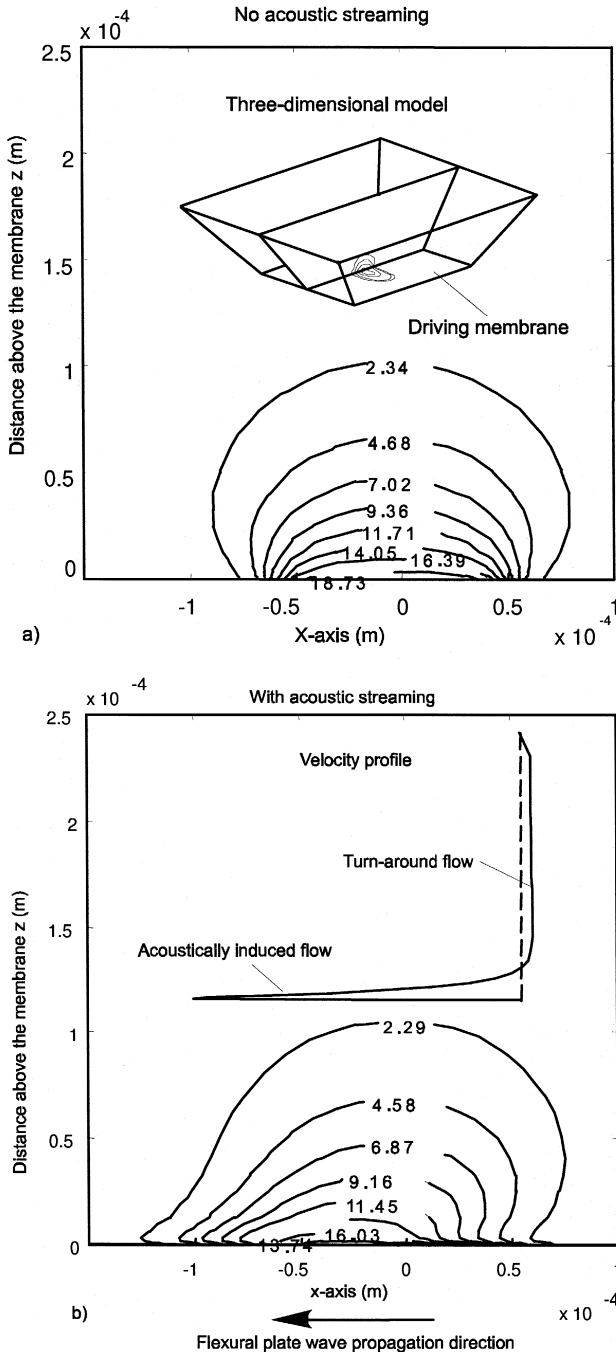


Fig. 5. Temperature profile in fluid without acoustic streaming (a) and with acoustic streaming (b).

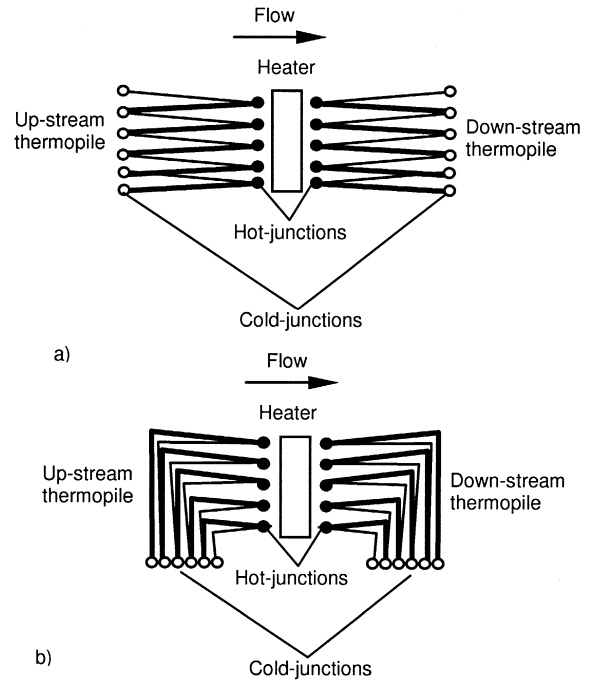


Fig. 6. Principle of the thermopile-heater-thermopile arrangement in a thermal flow sensor: (a) classical design, (b) new design for improvement of long-time stability.

Using the same simulation tool described above, the influence of the acoustic streaming on the temperature profile in the fluid can also be predicted. Fig. 5 shows the simulation results in a closed device using a three-dimensional model. The model shown in Fig. 5a has an actuating membrane at the bottom. All other sides of the model are set as walls. Since the device is closed, there is a turn-around flow at the top of the channel (Fig. 5b). Without the acoustic streaming, the temperature profile shown in Fig. 5a is symmetrical. With the acoustic streaming, the temperature profile indicates clearly the acoustic induced flow close to the actuating membrane, and the turn-around flow at the top of the channel (Fig. 5b).

The design of the flow sensor considers drift-effects of the thermal flow sensors based on thermopiles. In all published works, the cold junctions of thermopiles are located in the flow direction (Fig. 6a). That means the fluid transports the thermal energy directly from the heater to the cold junctions of the down-stream thermopiles. After a while in operation, the fluid will elevate the temperature of the cold junctions. This effect causes the drift of the sensor signal. In our design, the cold-junctions are located sideward, out of the influence of the thermal transfer (Fig. 6b). This new arrangement promises a better long-time behavior of the flow sensor.

### 3. Fabrication

The fabrication sequences for the microfluidic system are sketched in Fig. 7. Starting with a  $\langle 100 \rangle$  silicon wafer, the membrane was fabricated by coating a thick LPCVD

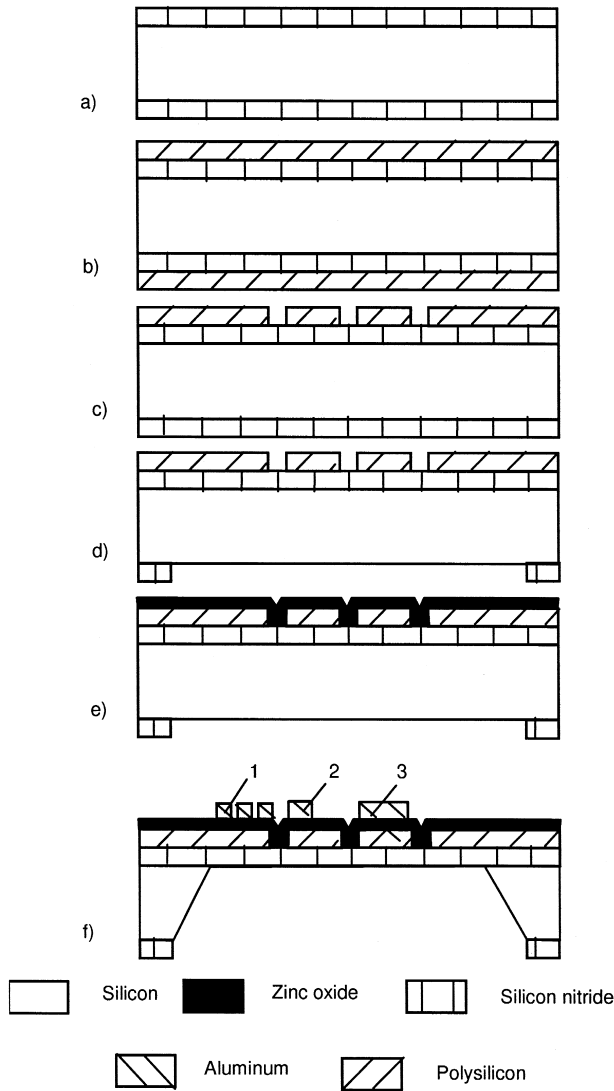


Fig. 7. Fabrication sequences of the micro fluidic system: (1) interdigitated electrode, (2) thermopile, (3) heater.

low-stress silicon nitride layer (Fig. 7a), and a polysilicon layer subsequently (Fig. 7b). The polysilicon layer was

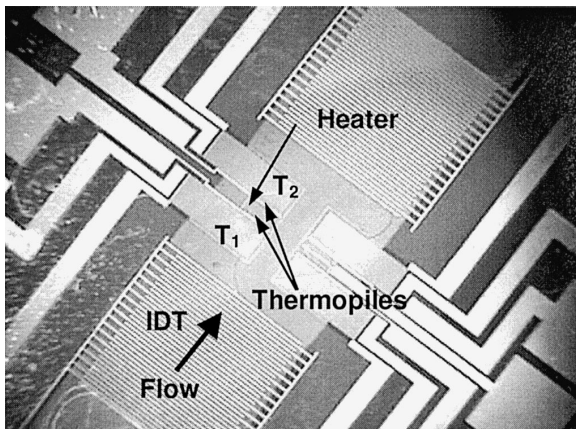


Fig. 8. The fabricated microfluidic system with integrated FPW pump and thermal low sensors.

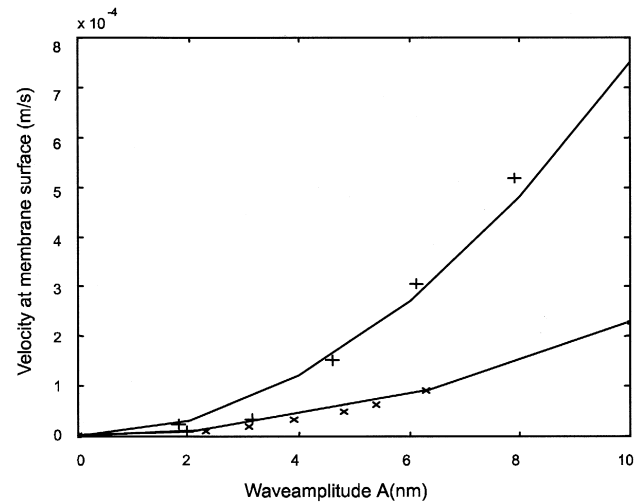


Fig. 9. Acoustic streaming velocities in water vs. wave amplitude. +: experimental results of 15- $\mu$ m channel,  $\times$ : experimental results of 500- $\mu$ m channel.

then patterned and etched in order to form the heater and the first part of the temperature sensors (Fig. 7c). Afterwards, the silicon nitride layer of the backside was opened with dry etching, in preparation for membrane formation (Fig. 7d). After the RF magnetron-sputtering of the zinc oxide layer, the contacts to the polysilicon were opened by patterning and etching the zinc oxide (Fig. 7e). Thereafter, aluminum was sputtered and structured in order to fabricate contacts to the heater, aluminum parts of the thermopiles and the interdigitated electrodes. Finally, the FPW membrane was freed by etching the silicon with KOH (Fig. 7f). The fabricated device is shown in Fig. 8.

#### 4. Experimental results

For validating the pumping performances, the device was tested with water. Flow velocity measurement was

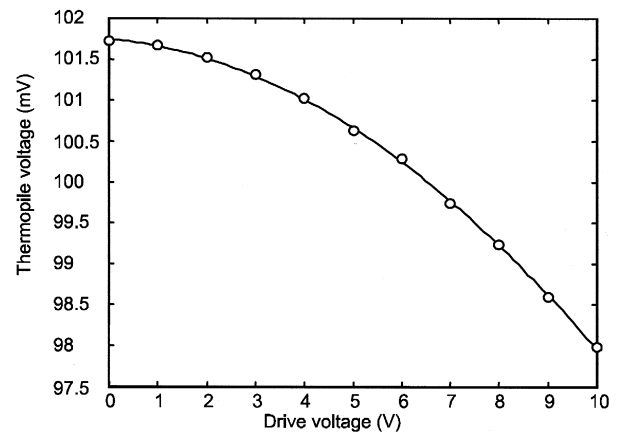


Fig. 10. Thermopile voltages (heater temperature) vs. drive voltages (wave amplitudes) in hot-film mode with 8.4 mW heat power (measurement in air).

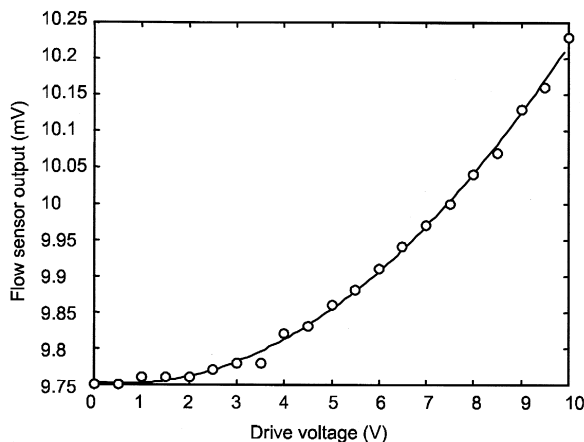


Fig. 11. Flow sensor signals (flow velocities) vs. drive voltages (wave amplitudes) in electrocaloric mode with 3.1 mW heat power (measurement in air).

carried out using 2- $\mu\text{m}$  polystyrene spheres in devices with 500- and 15- $\mu\text{m}$  channel height. Results in Fig. 9 show the velocities of the spheres has the quadratic behavior as expected in the numerical simulation (see Fig. 3). The solid lines in Fig. 9 indicate the simulation results that are corrected by factor 7 in order to fit the slower particle velocities. The wave amplitude was measured using the laser diffraction method [6]. Second, the thermopile performance was characterized. The results showed a linear behavior of the thermopile output.

The performance of the flow sensor and the FPW pump was then tested in air. The device was protected with a cover in order to minimize airflow from the surrounding environment. The heat power was kept under 10 mW because of the disturbance of the turbulent free convection at high temperature.

The thermal flow sensor was operated in two modes: the hot-film mode and the electrocaloric mode [12]. In the hot-film mode, the cooling of the heater at a constant heating power was measured. The heater temperature gives information about the flow. In the electrocaloric mode, the difference in fluid temperature up- and downstream of the heater  $T_2 - T_1$  (Fig. 8) indicates the bypassing flow. Fig. 10 illustrates the temperature of the heater's left side vs. the drive voltages of the IDTs at a constant heating power. The cooling characteristics have a typical quadratic behavior.

In the electrocaloric mode, the voltage difference between thermopiles up- and downstream of the heater is used as the sensor signal. For low flow rates, the sensor signals is proportional to the flow velocity [12]. The sensor output–drive voltage characteristics are shown in Fig. 11. The flow velocity–wave amplitude characteristics have a quadratic behavior. In both Figs. 10 and 11, circles are measurement points, lines are fitting curves.

## 5. Conclusions

We have presented and proven the performance of a thermal flow sensor integrated in an FPW device for in situ measurement and control of acoustic streaming. The acoustically driven micropump offers the advantages of low operating voltages and gentle pumping with no valves involved. The pump is especially suitable for delivering cells and other sensitive biomaterials. The thermal flow sensor described in this paper is able to detect the relatively slow velocity of the acoustic streaming. Further calibration works should be carried out in order to use the sensor for detecting the small volume flow rate. The experimental results show the possibility of a closed-loop-controlled system, which has many applications. Potential applications include reagent transport in a micro total analysis system ( $\mu\text{TAS}$ ), cell manipulating systems, and drug delivery systems.

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